

Deep learning-based automatic-bone-destruction-evaluation system using contextual information from other joints

美山, 和毅

<https://hdl.handle.net/2324/6787468>

出版情報 : 九州大学, 2022, 博士 (医学), 課程博士
バージョン :

権利関係 : (c) The Author(s) 2022. Open Access This article is licensed under a Creative Commons Attribution 4.0 International License



RESEARCH

Open Access



Deep learning-based automatic-bone-destruction-evaluation system using contextual information from other joints

Kazuki Miyama^{1,2*}, Ryoma Bise², Satoshi Ikemura¹, Kazuhiro Kai¹, Masaya Kanahori¹, Shinkichi Arisumi¹, Taisuke Uchida¹, Yasuharu Nakashima¹ and Seiichi Uchida²

Abstract

Background: X-ray images are commonly used to assess the bone destruction of rheumatoid arthritis. The purpose of this study is to propose an automatic-bone-destruction-evaluation system fully utilizing deep neural networks (DNN). This system detects all target joints of the modified Sharp/van der Heijde score (SHS) from a hand X-ray image. It then classifies every target joint as intact (SHS = 0) or non-intact (SHS $\geq$ 1).

Methods: We used 226 hand X-ray images of 40 rheumatoid arthritis patients. As for detection, we used a DNN model called DeepLabCut. As for classification, we built four classification models that classify the detected joint as intact or non-intact. The first model classifies each joint independently, whereas the second model does it while comparing the same contralateral joint. The third model compares the same joint group (e.g., the proximal interphalangeal joints) of one hand and the fourth model compares the same joint group of both hands. We evaluated DeepLabCut's detection performance and classification models' performances. The classification models' performances were compared to three orthopedic surgeons.

Results: Detection rates for all the target joints were 98.0% and 97.3% for erosion and joint space narrowing (JSN). Among the four classification models, the model that compares the same contralateral joint showed the best F-measure (0.70, 0.81) and area under the curve of the precision-recall curve (PR-AUC) (0.73, 0.85) regarding erosion and JSN. As for erosion, the F-measure and PR-AUC of this model were better than the best of the orthopedic surgeons.

Conclusions: The proposed system was useful. All the target joints were detected with high accuracy. The classification model that compared the same contralateral joint showed better performance than the orthopedic surgeons regarding erosion.

Keywords: Rheumatoid arthritis, Deep neural networks, Modified Sharp/van der Heijde score, Automatic detection, Automatic classification

Introduction

Assessing the presence of bone destruction is important for diagnosing rheumatoid arthritis (RA) [1, 2]. In clinical settings, bone destruction is usually estimated as accurately as possible by observing X-ray images [3]. If the X-ray images reveal signs of bone destruction, the chance of an RA diagnosis is significantly increased, and early drug treatment is more likely to be suggested [4].

*Correspondence: kazuki.miyama@human.ait.kyushu-u.ac.jp

² Department of Advanced Information Technology, Kyushu University, 744 Motoooka, Nishi-Ku, Fukuoka 819-0395, Japan
Full list of author information is available at the end of the article



© The Author(s) 2022. **Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>. The Creative Commons Public Domain Dedication waiver (<http://creativecommons.org/publicdomain/zero/1.0/>) applies to the data made available in this article, unless otherwise stated in a credit line to the data.

The modified Sharp/van der Heijde score (SHS) [5] is a commonly used metric for evaluating bone destruction by X-rays [6–8]. SHS has two assessment items: erosion and joint space narrowing (JSN). Erosion is assessed in 16 joints and JSN is assessed in 15 joints for each hand and wrist. SHS for erosion has six grades from 0 to 5, and SHS for JSN has five grades from 0 to 4 [5].

Among the grades, the classification between 0 (intact) and the others (non-intact) is the most important task for early diagnosis of RA [6]. However, performing this binary classification by visual inspection is difficult, even for RA experts, for three reasons.

First, binary classification of all joints by visual inspection is time-consuming [1, 9–11]. Second, accurate and stable classification requires extensive practical experience. Third, although each RA expert attempts the classification to the best of their ability, it is hard to avoid intra- and inter-expert variability. These three problems make it difficult to perform binary classification in actual clinical practice.

The purpose of this study is to propose a system for automatically evaluating bone destruction (hereafter, “automatic-bone-destruction-evaluation system”) by fully utilizing recent artificial intelligence (AI) techniques, called deep neural networks (DNN). The system first detects all target joints from a single X-ray image of the hands. It then classifies every target joint as “intact” (SHS = 0) or “non-intact” (SHS ≥ 1).

The contributions of this study are twofold. First, the proposed system is the first that can detect all the target joints automatically. As for methods developed in previous studies [12–14], the change in brightness is used to detect the target joints. Due to their complex structure, the target joints were limited to proximal interphalangeal (PIP), interphalangeal joint of the thumb (IP), and metacarpophalangeal (MCP) joints [12–14]. To detect all the target joints, we introduced a DNN model called *DeepLabCut*, which can detect

various objects accurately by re-training the model with different targets [15].

Second, the proposed system is the first that performs binary classification for each joint while utilizing “contextual” information from other joints. As for RA, bone destruction progresses bilaterally and symmetrically [1, 3, 16–18]. Therefore, comparing both hands is useful when reading X-ray images of RA patients [9, 19–21]. Furthermore, the bone destruction of the same joint group, such as the PIP joints, tends to progress similarly [22, 23]. These comparisons of the related joints are often used in diagnosing RA. Therefore, we propose a method that evaluates the target joints using information concerning the relevant joints.

Materials and methods

Dataset

The Institutional Review Board approved this study. We used 226 hand X-ray images from 40 patients diagnosed with RA and treated with medication from 2008 to 2019 in nine hospitals (Fig. 1). Table 1 shows patients’ characteristics and breakdowns between hospitals. All X-rays contained the target joints completely. There were no images that were excluded by the image quality. Three orthopedic surgeons who treat RA attached the ground-truth (GT) for each target joint as “intact” or “non-intact” by consensus (Fig. 1). The numbers of intact and non-intact GTs for each joint are given in Table 2. Some joints are biased to be intact or non-intact, and this bias, called “class imbalance,” adversely affects the prediction performance of the DNN [24]. We applied the data augmentation [25] described below to mitigate this class imbalance.

Method (overview)

Figure 2 overviews the proposed automatic-bone-destruction-evaluation system, which consists of three steps. First, a detection model detects the center point of the target joints (16 joints for erosion and 15 joints for

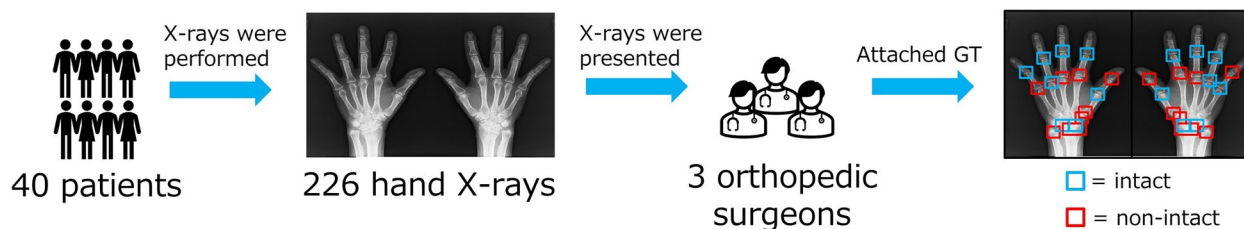


Fig. 1 The flow of how the dataset was generated. The subjects of this study were 40 rheumatoid arthritis patients treated from 2008 to 2019 in 9 hospitals. All patients have both hands X-rayed. X-rays were taken at intervals of at least 1 year when more than one radiograph was taken for a single patient; 3 patients were X-rayed once, 5 patients were X-rayed twice, 30 patients were X-rayed 3 times, 1 patient was X-rayed 4 times, and 1 patient was X-rayed 6 times. In total, there were 113 both hands X-rays (i.e., 226 one-hand X-rays). Three orthopedic surgeons were presented with full hand X-rays and attached the ground-truth (GT) for each target joint as “intact” or “non-intact” by consensus

Table 1 Patients' characteristics for each hospital

	Site 1 n = 3	Site 2 n = 1	Site 3 n = 2	Site 4 n = 14	Site 5 n = 2	Site 6 n = 2	Site 7 n = 1	Site 8 n = 1	Site 9 n = 14	All n = 40
Age (years)	61.3 ± 16.1	71.0 ± 0.0	63.0 ± 0.0	60.0 ± 10.1	73.5 ± 4.5	57.0 ± 9.0	73.0 ± 0.0	70.0 ± 0.0	59.5 ± 12.6	61.5 ± 11.6
Sex (male: female)	0: 3	0: 1	0: 2	2: 12	0: 2	0: 2	0: 1	0: 1	2: 12	4: 36
RA duration (years)	10.7 ± 9.5	N/A	14.0 ± 11.0	6.5 ± 4.6	20.0 ± 19.0	9.5 ± 1.5	13.0 ± 0.0	9.0 ± 0.0	15.1 ± 10.0	11.4 ± 9.7
MTX	3 (100%)	1 (100%)	2 (100%)	12 (86%)	1 (50%)	1 (50%)	1 (100%)	1 (100%)	11 (79%)	33 (83%)
Glucocorticoids	1 (33%)	1 (100%)	1 (50%)	13 (93%)	2 (100%)	2 (100%)	1 (100%)	0 (0%)	5 (36%)	26 (66%)
bDMARDs	2 (67%)	0 (0%)	1 (50%)	6 (43%)	0 (0%)	0 (0%)	1 (100%)	1 (100%)	9 (64%)	20 (50%)

Patients' characteristics for each hospital are shown. Age and rheumatoid arthritis (RA) data represent average ± SD

RA rheumatoid arthritis, MTX methotrexate, bDMARDs biologic disease-modifying anti-rheumatic drugs

Table 2 Breakdown of the number of intact or non-intact images for each target joint

	Intact	Non-intact	Total
Erosion			
PIP-IP	1005	125	1130
MCP	987	143	1130
CMC-M	321	131	452
Wrist	434	470	904
All joints	2747	869	3616
JSN			
PIP	562	342	904
MCP	876	254	1130
CMC	328	350	678
Wrist	217	461	678
All joints	1983	1407	3390

The number of intact or non-intact images for each target joint is shown. For erosion, "Wrist" represents the navicular, the lunate, the radius, and the ulna; for JSN, "Wrist" represents the multangular-navicular, the capitate-navicular-lunate, and the radiocarpal joint

PIP proximal interphalangeal, IP interphalangeal, MCP metacarpophalangeal, CMC-M carpometacarpal joint of the thumb and multangular, JSN joint space narrowing, CMC carpometacarpal

JSN) from an inputted hand X-ray image (Fig. 2A). Next, each joint image is cropped around the detected center point. The cropped image is then input into the classification model for binary classification (Fig. 2B).

Training of detection model

As the detection model, DeepLabCut [15], which was proposed for detecting and tracking an animal's joints in video images, was used. DeepLabCut estimates each key point (joint) position from an input image. This detection model has three advantages: first, it can be applied to various objects by re-training it with a different target; second, it can be trained with a few labeled training data; and third, it can detect joints accurately by learning the structure of the joints (e.g., mutual positional

relationships). We thus used DeepLabCut for detecting the target joints.

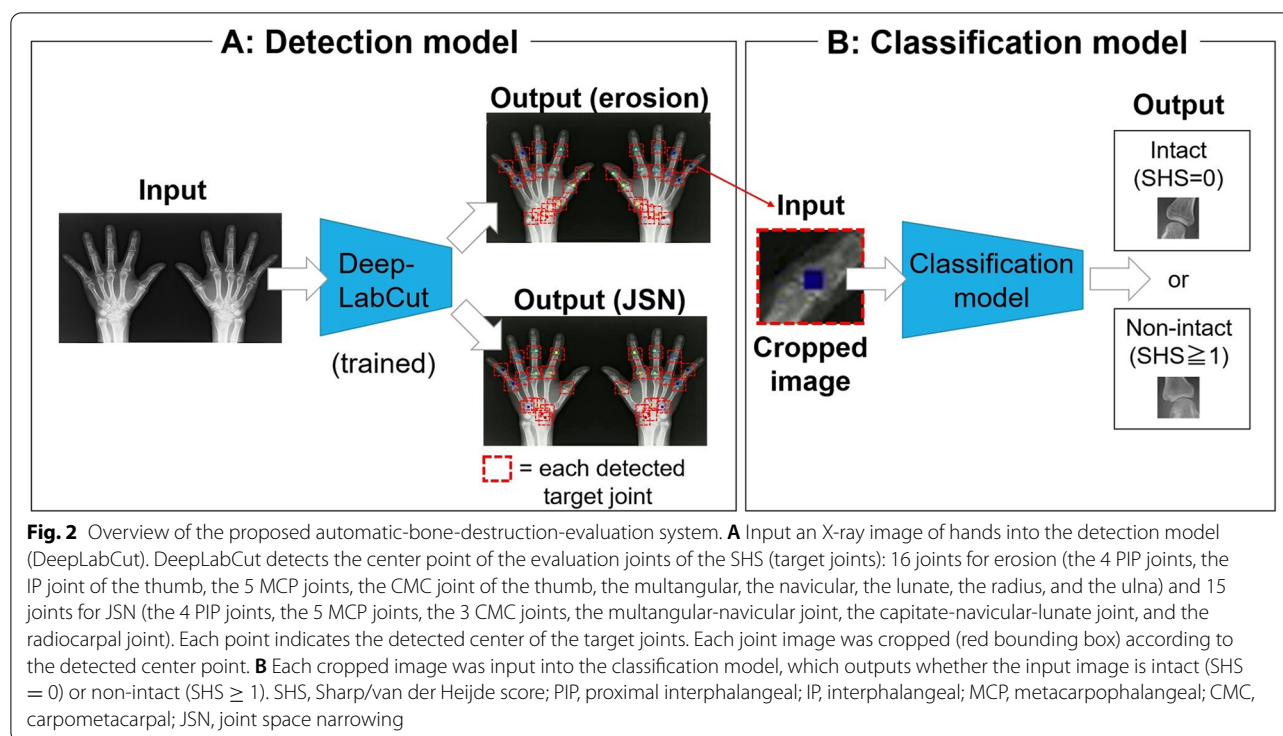
In the training of DeepLabCut, 20 X-ray images were randomly selected from 226 X-rays and resized to 256 × 256 pixels. Then, for each of the 20 images, the center points of the target joints were annotated by an orthopedic surgeon. Finally, two DeepLabCut models were trained with those training images: one to detect the target joints for erosion (16 joints) and the other to detect the target joints for JSN (15 joints).

Models for classification

Several binary classification models were established, and their performances were compared via experiments. Figure 3A shows the baseline model, called the single-input single-output (SISO) model. The SISO model is the simplest and classifies each detected joint independently. In other words, it does not utilize information concerning other joints. As the backbone of the SISO model, a VGG16 [26], which has a typical convolutional neural network [27] structure and high object-recognition performance, was used. It is well-known that pre-training a neural network model with a large but non-target dataset boosts its performance. The VGG16 was therefore pre-trained by ImageNet [28] and then fine-tuned [29] by using (a limited number of) joint images.

In addition to the SISO model, three types of multiple-input multiple-output (MIMO) models were established. As discussed in the introduction, it is effective to compare the same contralateral joint [9, 19–21] or the same joint group [22]. From this viewpoint, the SISO model has room for improvement because it does not use the information on the relevant joints. The established MIMO models utilize information about the same contralateral joint and joint group (Fig. 3B–D).

For designing the MIMO models, the same joint group in one hand is defined as follows (Fig. 3E): for erosion, (1) the PIP and IP joints (PIP-IP joints), (2) the MCP joints, (3) the carpometacarpal (CMC) joint of the thumb and



multangular (CMC-M), and (4) the wrist joints (the navicular, the lunate, the radius, and the ulna) [22, 23], and for JSN, (1) the PIP joints, (2) the MCP joints, (3) the CMC joints, and (4) the wrist joints (the multangular-navicular joint, the capitate-navicular-lunate joint, and the radiocarpal joint) [22, 23]. Given a set of joint images (the same joints of both hands or the same joint group) as inputs, the model simultaneously estimates the classes (“intact” or “non-intact”) of these multiple joints.

Figure 3B shows the *MIMO local* model, which can compare the same contralateral joint. This MIMO model receives inputs from the same joints of both hands and outputs “intact” or “non-intact” for each joint. Since the same (local) joints of both hands are compared, this model is referred to as the “MIMO local model.”

Figure 3C shows the *MIMO one-hand* model, which can compare multiple joints in the same joint group of one hand. This model gives all classification results for individual joints in their group using the mutual relationship.

Figure 3D shows the *MIMO both-hands* model, which can compare the same joint group of both hands. This model may take advantage of both the MIMO local model and the MIMO one-hand model.

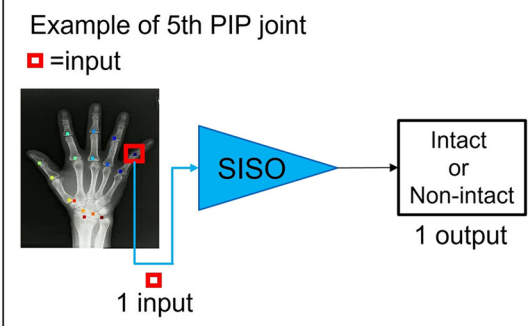
Training of classification models

The four classification models (SISO and three MIMOs) were trained under the following conditions. First, forty

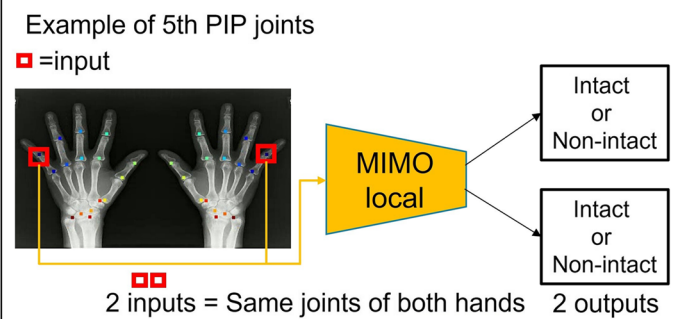
patients were divided into eight patient-disjoint subsets (i.e., five patients in each subset). This patient-disjointness is necessary to keep the fairness of our experiment [30]. Then, eightfold cross-validation was performed, where six subsets were used for training, one subset was used for validation, and one subset was used for testing. The classification models were trained by using the training images. The validation data was used to adjust hyperparameters and determine when to stop the training prematurely, namely, “early stopping,” which is used to improve the generalization of the test data [31].

The hyperparameters were as follows; the number of fully connected layers [32], the initialization scheme for fully connected layers (random or He normal initialization [33]), dropout [34], and batch size [35]. The hyperparameters were tuned to minimize the loss of validation data, and the final settings are described in Tables S1 and S2 in additional materials. The condition for early stopping was that validation loss does not decrease 10 times in a row. The training is terminated if this early stopping condition is not satisfied for 100 epochs. We set the binary cross-entropy loss [36] for the SISO model and the sum of the binary cross-entropy losses over all outputs for the MIMO models. The Adaptive Momentum (Adam) [37] was used as the optimizer for all models. Since image features among different joint groups differ significantly, different models were prepared for each group, as shown in Tables S1 and S2 in additional materials.

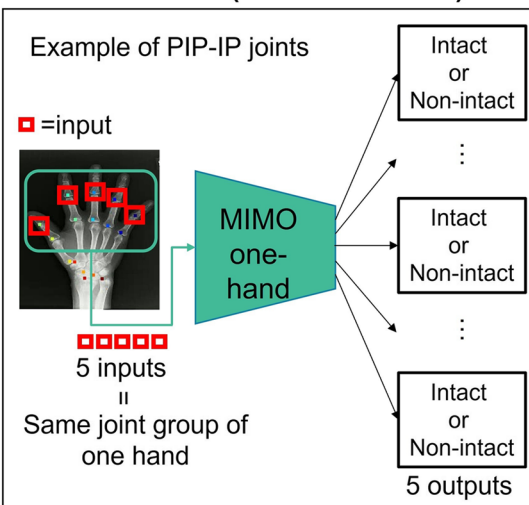
A: Single-input single-output model (SISO)



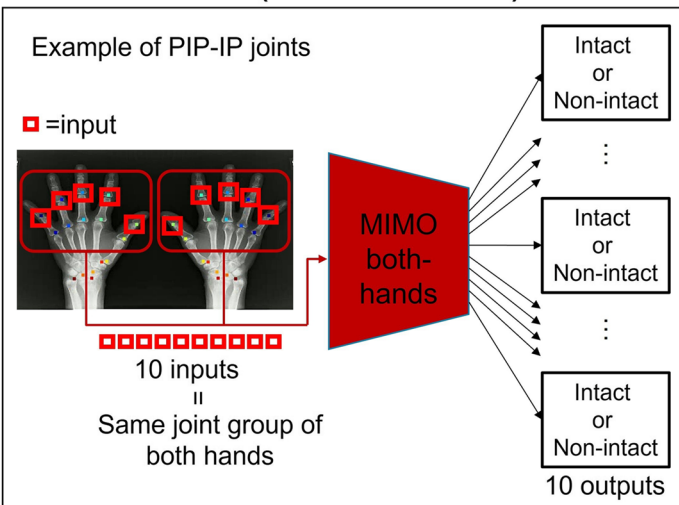
B: Multiple-input multiple-output model at a specific joint (MIMO local)



C: Multiple-input multiple-output model on one hand (MIMO one-hand)



D: Multiple-input multiple-output model on both hands (MIMO both-hands)



E: The same joint groups of erosion and JSN

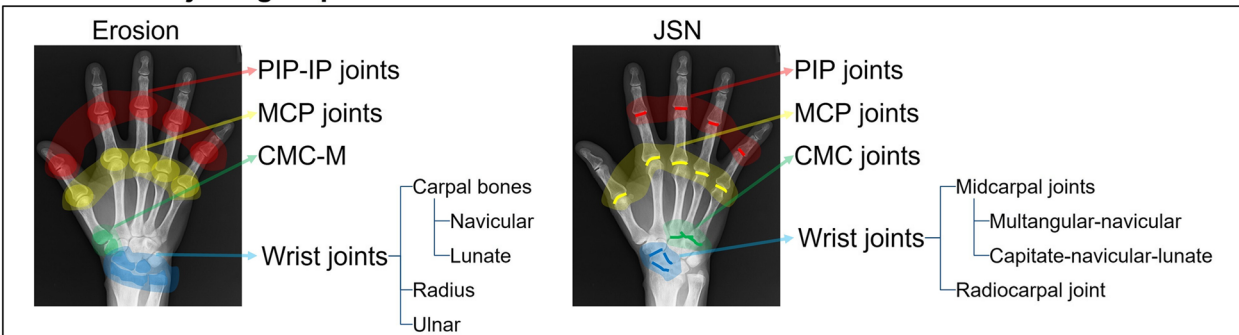


Fig. 3 Overview of the binary classification model and the same joint groups. We developed four classification models: **A** A most-basic classification model that independently classifies each joint as intact (SHS = 0) or non-intact (SHS ≥ 1) (single-input single-output model). **B** A classification model that inputs the same joints of both hands and outputs intact or non-intact, respectively (multiple-input multiple-output model at a specific joint). **C** A classification model that receives inputs of the same joint group of one hand and outputs whether they are intact or non-intact, respectively (multiple-input multiple-output model on the one hand). **D** A classification model that receives inputs of the same joint group of both hands and outputs, whether intact or non-intact, respectively (multiple-input multiple-output model on both hands). **E** The same joint groups of both hands for erosion and JSN. PIP, proximal interphalangeal; IP, interphalangeal; MCP, metacarpophalangeal; CMC-M, carpometacarpal joint of the thumb and multangular; CMC, carpometacarpal

To address the class imbalance, we applied data augmentation, which improves the performance of the DNN when there is a class imbalance or only a small amount of training data [25]. We applied data augmentation to the training and validation data (for each joint of each fold in the cross-validation). Specifically, we applied -3- to 3-degrees rotations, -5- to 5-pixels vertical and horizontal translations, and 0.97- to 1.03-times enlargement (or reductions) to each cropped joint image. The geometric perturbations augmented the training data until the total number of images was about 10,000 with no class imbalance. The validation data were also augmented to remove the class imbalance.

Procedure for evaluation of detection model

The performance of DeepLabCut was evaluated in the following two metrics using 206 test X-ray images: (1) the correct detection rate: the number of correct detections divided by the total number of joints and (2) the distance error: the Euclidian distance (in pixels) of the detected center of the target joint from the GT coordinates. Since the X-ray images and hands have various scales and sizes, the X-ray images were first resized so that all images' median lengths of the proximal phalanges matched. Next, bounding boxes were formed around the detected center points. The box sizes are 250×250 pixels for the PIP, IP, MCP, and CMC-M joints, 500×300 pixels for the radius, and 300×300 pixels for the others. For the correct detection rate, an orthopedic surgeon checked whether the bounding box correctly contained the target joint. If not, the box is treated as an error and discarded from the later experiment. For distance error, an orthopedic surgeon annotated the GT coordinate of the center of all target joints of both erosion and JSN for 50 X-ray images selected randomly from 206 test images. Then, the Euclidian distance of the detected target joint's center from the GT coordinates was evaluated.

Procedure for evaluation of classification models

The performance of the proposed four classification models was evaluated by using sensitivity, specificity, F-measure [38], and PR-AUC [39] with eightfold cross-validation. F-measure and PR-AUC are important indicators of classification model performance when there is a class imbalance [40, 41], as in this study. F-measure is the harmonic mean of sensitivity and precision, and PR-AUC is the curve of the area under the precision-recall curve, which is a plot of precision against sensitivity. F-measure and PR-AUC take values between 0 and 1 and become closer to 1 as performance improves.

Binary classification performance of the three orthopedic surgeons who were different from those who attached GT was also tested using the same 226 X-rays. These

three orthopedic surgeons were not experts in RA. They evaluated each target joint for erosion and JSN as "intact" or "non-intact."

Results

Joint detection results

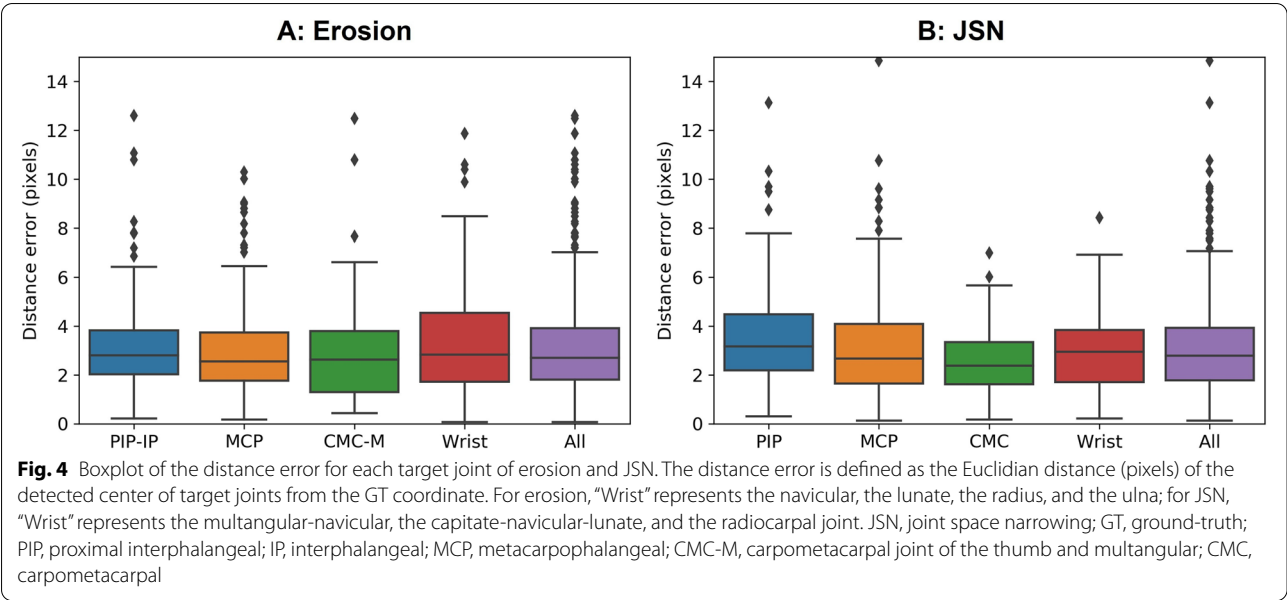
Table 3 shows the correct detection rates for each target joint. The detection rates for each joint are as follows (intact, non-intact, total): for erosion, the PIP-IP joints (99.5%, 90.8%, 98.5%), the MCP joints (99.6%, 83.1%, 97.5%), the CMC-M (99.3%, 93.4%, 97.6%), the wrist joints (100.0%, 96.3%, 98.1%), and all joints (99.6%, 92.9%, 98.0%), and for JSN, the PIP joints (99.0%, 91.6%, 96.2%), the MCP joints (98.2%, 86.8%, 95.6%), the CMC joints (99.7%, 98.7%, 99.2%), the wrist joints (100.0%, 99.8%, 99.8%), and all joints (98.9%, 95.2%, 97.3%). On the whole, all the target joints were detected with high accuracy. Intact joints (SHS = 0) were detected correctly in most cases. Detection performance was generally good in the case of non-intact joints (SHS ≥ 1), although detection rates for the PIP-IP and MCP joints tended to be a little low for both erosion and JSN.

Figure 4 shows that the average distance errors were less than 6 pixels for all target joints for both erosion and JSN. The distance error for each joint are as follows (average $\pm$ SD pixels): for erosion, the PIP-IP joints (3.4 ± 3.5), the MCP joints (3.0 ± 2.6), the CMC-M (3.1 ± 2.9), the wrist joints (3.7 ± 4.1), and all joints (3.3 ± 3.4), and for JSN, the PIP joints (5.4 ± 9.4), the MCP joints ($3.8 \pm$

Table 3 Correct detection rates for test data

	Intact	Non-intact	Total
Erosion			
PIP-IP	916/921 (99.5%)	99/109 (90.8%)	1015/1030 (98.5%)
MCP	896/900 (99.6%)	108/130 (83.1%)	1004/1030 (97.5%)
CMC-M	289/291 (99.3%)	113/121 (93.4%)	402/412 (97.6%)
Wrist	393/393 (100.0%)	415/431 (96.3%)	806/824 (98.1%)
All joints	2494/2505 (99.6%)	735/791 (92.9%)	3229/3296 (98.0%)
JSN			
PIP	508/513 (99.0%)	285/311 (91.6%)	793/824 (96.2%)
MCP	782/796 (98.2%)	203/234 (86.8%)	985/1030 (95.6%)
CMC	304/305 (99.7%)	309/313 (98.7%)	613/618 (99.2%)
Wrist	197/197 (100.0%)	420/421 (99.8%)	617/618 (99.8%)
All joints	1791/1811 (98.9%)	1217/1279 (95.2%)	3008/3090 (97.3%)

Correct detection rates for intact (SHS = 0) joints, non-intact (SHS ≥ 1) joints, and the total for each target joint are shown. The numbers represent the correct detection/total cases (correct detection rates %). In erosion, "Wrist" represents the navicular, the lunate, the radius, and the ulna. In JSN, "Wrist" represents the multangular-navicular, the capitate-navicular-lunate, and the radiocarpal joint. GT ground-truth, PIP proximal interphalangeal, IP interphalangeal, MCP metacarpophalangeal, CMC-M carpometacarpal joint of the thumb and multangular, JSN joint space narrowing, CMC carpometacarpal



6.5), the CMC joints (2.5 ± 1.2), the wrist joints (2.9 ± 1.5), and all joints (3.8 ± 6.3).

Figure 5 shows examples of joint detection. In Fig. 5A, joints with no or moderate bone destruction were successfully detected. In Fig. 5B, in the case of severe bone destruction, false positives (yellow arrows) and false negatives (red arrows) for PIP and MCP joints were observed. On the contrary, the wrist joints could be

detected accurately for both erosion and JSN, even when severe bone destruction was present.

Results (classification)

Table 4 shows the binary classification performance of each classification model and each orthopedic surgeon for three groups (the wrist joints, the others, and all joints [the wrist joints and the others]). For all joints, in

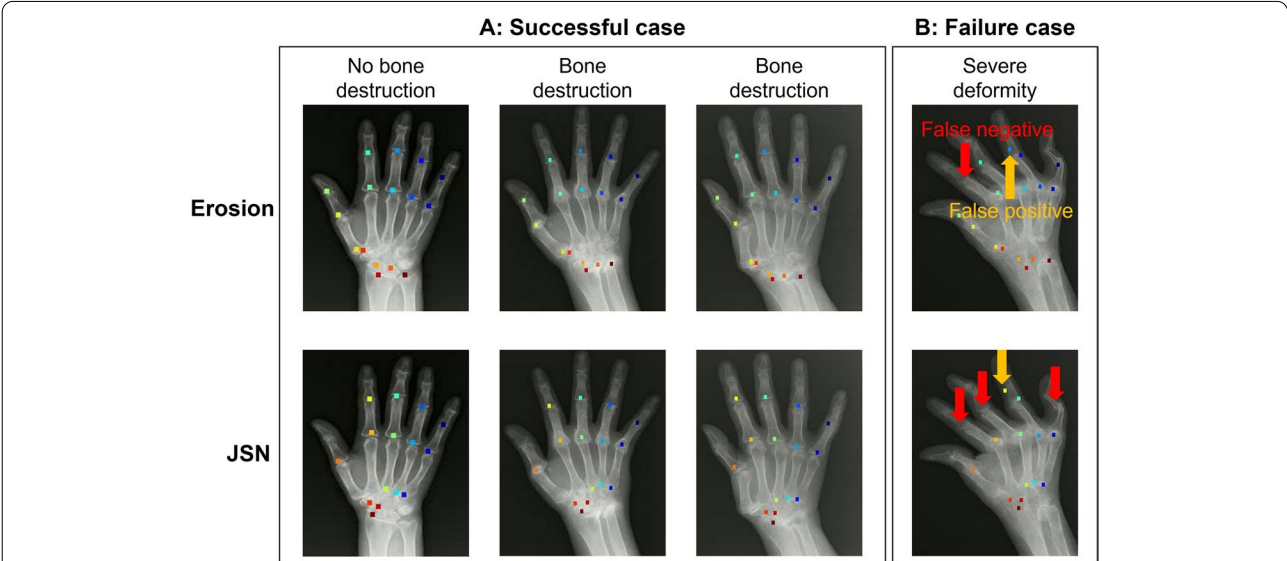


Fig. 5 Detection results by DeepLabCut. Each point means the detected center point of the target joints, and each color corresponds to each joint. **A** DeepLabCut could detect the joints with high accuracy in cases with or without moderate bone destruction. **B** Detection failed in cases of severe bone destruction. The yellow arrow shows DeepLabCut detected the wrong area (false positive). The red arrow shows DeepLabCut could not detect the target joints (false negative)

Table 4 Performance of binary classification

	SISO	MIMO local	MIMO one-hand	MIMO both-hands	Orthopedic surgeon 1	Orthopedic surgeon 2	Orthopedic surgeon 3	Average of surgeons
PIP-IP+MCP+ CMC-M (erosion)								
Sensitivity	0.65	0.54	0.51	0.31	0.64	0.94	0.93	0.84
Specificity	0.88	0.93	0.93	0.96	0.92	0.57	0.78	0.76
F-measure	0.50	0.52	0.50	0.38	0.57	0.36	0.51	0.48
PR-AUC	0.55	0.54	0.53	0.44	0.59	0.58	0.65	0.61
Wrist (erosion)								
Sensitivity	0.78	0.85	0.84	0.77	0.46	0.98	0.88	0.77
Specificity	0.86	0.85	0.83	0.88	0.95	0.30	0.65	0.64
F-measure	0.81	0.84	0.83	0.81	0.61	0.70	0.77	0.70
PR-AUC	0.86	0.88	0.87	0.87	0.81	0.77	0.81	0.80
All joints (erosion)								
Sensitivity	0.73	0.72	0.70	0.58	0.57	0.96	0.87	0.80
Specificity	0.88	0.92	0.92	0.95	0.93	0.53	0.77	0.74
F-measure	0.66	0.70	0.69	0.65	0.61	0.51	0.63	0.58
PR-AUC	0.69	0.73	0.72	0.70	0.66	0.66	0.70	0.67
PIP+MCP+CMC (JSN)								
Sensitivity	0.75	0.74	0.73	0.67	0.55	0.90	0.84	0.76
Specificity	0.84	0.90	0.89	0.88	0.93	0.83	0.87	0.88
F-measure	0.72	0.76	0.74	0.70	0.65	0.80	0.79	0.74
PR-AUC	0.76	0.81	0.79	0.75	0.74	0.82	0.82	0.79
Wrist (JSN)								
Sensitivity	0.81	0.87	0.83	0.84	0.80	0.98	0.91	0.90
Specificity	0.79	0.78	0.80	0.81	0.84	0.67	0.84	0.78
F-measure	0.85	0.88	0.86	0.87	0.85	0.91	0.91	0.89
PR-AUC	0.91	0.93	0.92	0.93	0.91	0.92	0.94	0.92
All joints (JSN)								
Sensitivity	0.77	0.79	0.77	0.74	0.62	0.93	0.86	0.80
Specificity	0.83	0.89	0.88	0.87	0.92	0.81	0.86	0.87
F-measure	0.76	0.81	0.79	0.76	0.71	0.84	0.83	0.80
PR-AUC	0.81	0.85	0.83	0.82	0.81	0.86	0.86	0.84

The performance of each classification model and orthopedic surgeons for erosion and JSN are shown. For erosion, "Wrist" represents the navicular, the lunate, the radius, and the ulna. For JSN, "Wrist" represents the multangular-navicular, the capitate-navicular-lunate, and the radiocarpal joint

SISO single-input single-output model, MIMO multiple-input multiple-output, JSN joint space narrowing, PR-AUC precision-recall area under the curve, PIP proximal interphalangeal, IP interphalangeal, MCP metacarpophalangeal, CMC-M carpometacarpal joint of thumb and multangular, CMC carpometacarpal

the case of both erosion and JSN, the MIMO local model and the MIMO one-hand model outperformed the SISO model in terms of F-measure and PR-AUC. Figure 6 shows the PR-curve. In addition, for all joints, the MIMO local model showed the best performance in terms of the following metrics: sensitivity of JSN (0.79), specificity of JSN (0.89), F-measure of erosion and JSN (0.70, 0.81), and PR-AUC of erosion and JSN (0.73, 0.85).

Furthermore, as for the F-measure and PR-AUC in the case of all joints, the MIMO local model showed better erosion classification performance than the best orthopedic surgeon. For JSN, this model was still better than the average of the orthopedic surgeons. For all joints,

F-measure and PR-AUC were as follows (MIMO local model, average of the orthopedic surgeons, best of the orthopedic surgeons): F-measure (0.70, 0.58, 0.63) and PR-AUC (0.73, 0.67, 0.70) for erosion and F-measure (0.81, 0.80, 0.84) and PR-AUC (0.85, 0.84, 0.86) for JSN.

Figure 7 shows examples of the visualization results of prediction by each classification model. In Fig. 7A, the MIMO local model correctly classified the left hand's navicular, lunate, and radius as non-intact, although the other models misrecognized them. For JSN, the MIMO local model correctly classified the right hand's radiocarpal joint and the left hand's CMC joints as non-intact, although the other models misrecognized them (Fig. 7B).

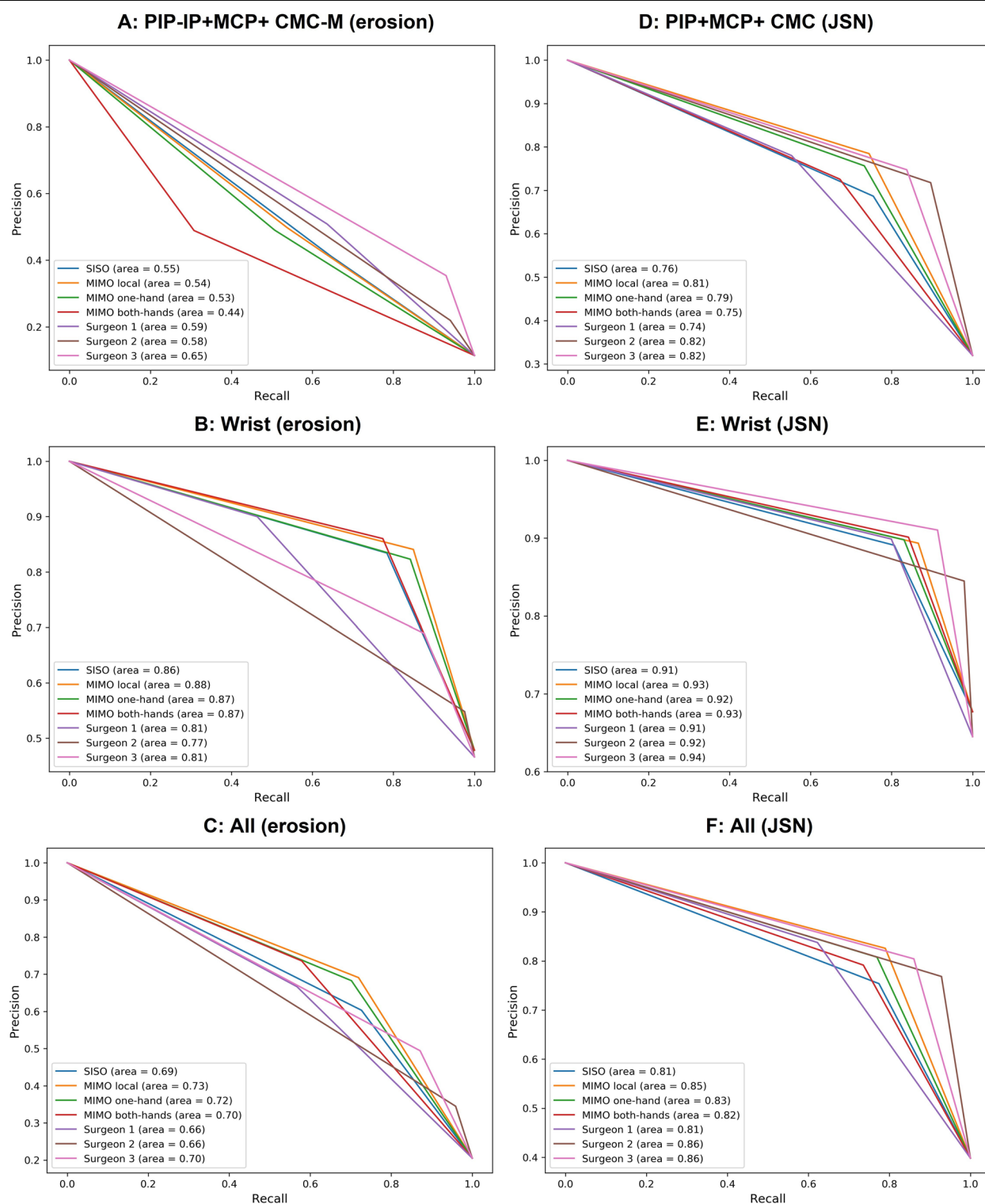


Fig. 6 Precision-recall curve and area under the curve of each classification model and orthopedic surgeon for each target joint. For erosion, “Wrist” represents the navicular, the lunate, the radius, and the ulna; for JSN, “Wrist” represents the multangular-navicular, the capitate-navicular-lunate, and the radiocarpal joint. JSN, joint space narrowing; GT, ground-truth; PIP, proximal interphalangeal; IP, interphalangeal; MCP, metacarpophalangeal; CMC-M, carpometacarpal joint of the thumb and multangular; CMC, carpometacarpal; SISO, single-input single-output; MIMO, multiple-input multiple-output

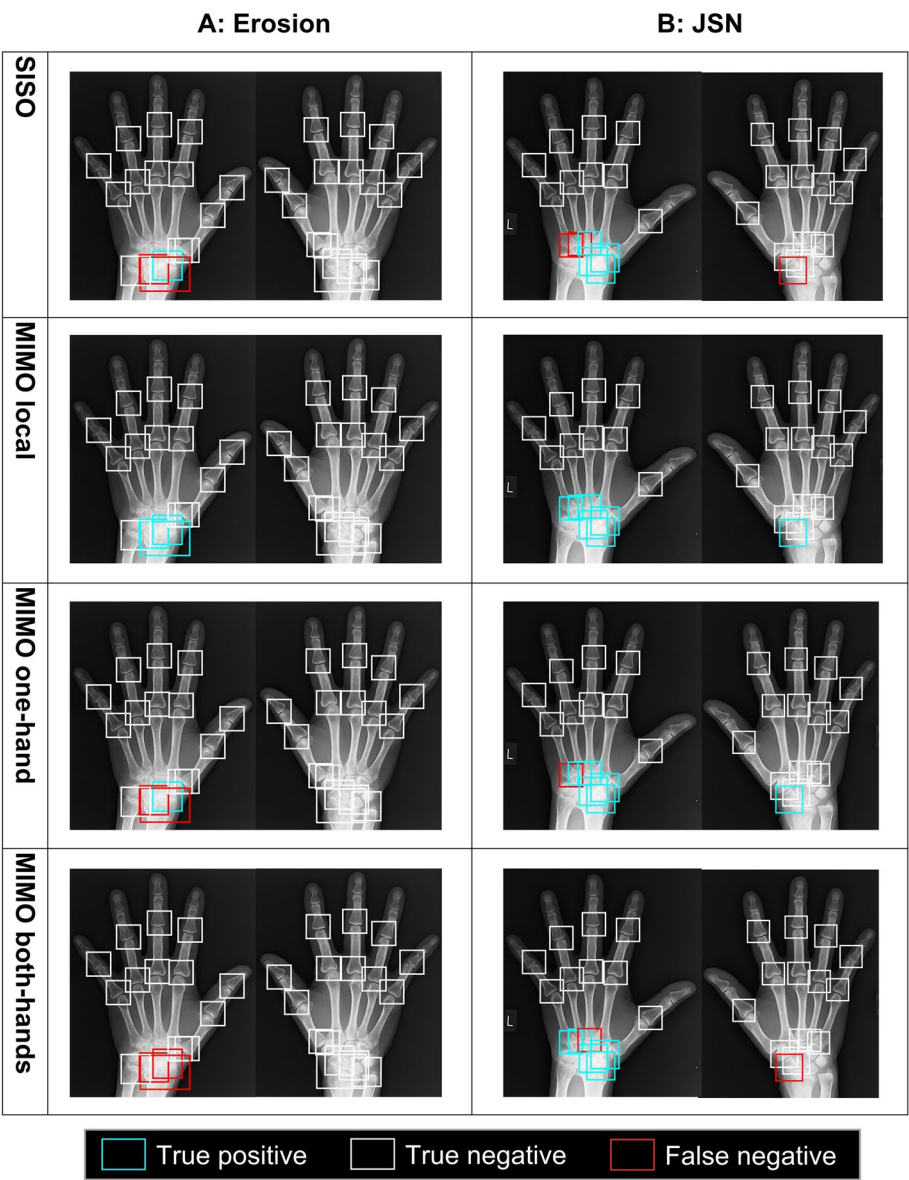


Fig. 7 Visualization results of prediction by each classification model of target joints in X-ray images. Each bounding box represents the detected target joints. The color of the bounding box indicates how the classification results compare to ground-truth (GT). Blue indicates GT is non-intact, and prediction is non-intact (true positive). White indicates GT is intact, and prediction is intact (true negative). Red indicates GT is non-intact, and prediction is intact (false negative). **A** The results for erosion and **B** for JSN. GT, ground-truth; JSN, joint space narrowing; SISO, single-input single-output; MIMO, multiple-input multiple-output

Discussion

The joint-detection performance of the proposed automatic-bone-destruction-evaluation system was very high for all the target joints. As for the binary classification, the MIMO local model, which could compare the same contralateral joint, showed the best performance for erosion and JSN regarding the F-measure and PR-AUC among the four classification models. In addition, the performance of

this model for erosion was higher than that of the orthopedic surgeons. The MIMO local model’s classification performance of JSN was slightly lower than that of the best orthopedic surgeon but was slightly better than the average of the orthopedic surgeons. Since erosion is more critical than JSN for early diagnosis of RA [42], it has a clinical significance that the MIMO local model outperformed the orthopedic surgeon’s performance on erosion.

As for automatic detection, all the target joints could be detected very accurately, as shown in Table 3. Past reports [12, 14] focused on changes in brightness values for automatic detection. These methods are effective when the joint space is well defined, such as in the PIP-IP and MCP joints, but it is ineffective in the case of anatomically complex structures such as the navicular and lunate [12, 14]. DeepLabCut accurately detected all the target joints by learning the anatomical position and relationship between each target joint. Furthermore, DeepLabCut's detection rates were better than previous reports [12, 14], although a direct comparison is difficult under different datasets. Hirano et al. [12] reported detection rates of 96.0% for the PIP-IP joints and 94.0% for the MCP joints. Morita et al. reported a detection rate of 91.8% for the 28 joints of the PIP joints, distal IP joints, and MCP joints. DeepLabCut's detection rates were 98.5% for the PIP-IP joints, 97.5% for the MCP joints, and 98.0% for the PIP-IP and MCP joints (Table 3). DeepLabCut showed higher detection performance of the PIP-IP and MCP joints than the previous reports [12, 14].

When ulnar drift occurs in the PIP and MCP joints (Fig. 5B), detection by the proposed system tends to fail. This tendency can be explained by a change in the anatomical positional relationship between the proximal phalanges and the metacarpal bone. In contrast, the wrist joints could be appropriately detected, even though RA had progressed, because they had less anatomical deviation than the finger joints [43].

As for binary classification, the MIMO local model achieved the best performance among the four classification models. Comparing the same contralateral joint was more effective than comparing the same joint group. Previous studies [16, 42] reported that comparing contralateral joints improves the performance of reading X-ray images and many rheumatologists have used this comparison technique to diagnose bone destruction. Although the MIMO both-hands model also compares joints of both hands, its performance was not better than that of the MIMO local model and the MIMO one-hand model. We consider that increasing the number of input joints requires a combinatorial increase of training data, so it makes sufficient training difficult. Thus, selecting effective input images for a classification model is necessary.

In the non-intact cases, the MIMO local model and the MIMO one-hand model were effective in the wrist joints for both erosion and JSN. Bone destruction of the wrist joints progresses more symmetrically than the finger joints [16, 44]; therefore, the MIMO local model was suitable for the wrist joints. The MIMO one-hand

model was also effective in the wrist joints because the group of the wrist joints had a similar progression of bone destruction.

In the case of mild bone destruction in erosion, which is important for early diagnosis [42], the four classification models showed relatively good performance for the wrist joints but not for the PIP-IP, MCP, and CMC-M joints. Figure 8 shows a difficult case for all four classification models. In the wrist joints of Fig. 8, 4 classification models could classify as non-intact correctly for almost all. However, all classification models misclassified the PIP and MCP joints as intact. These misclassifications could be explained by the mild degree of bone destruction. It is even difficult for rheumatologists to accurately discriminate between intact bone and mild bone destruction [45]. The classification models may therefore have difficulty in learning features that discriminate between intact bone and mild bone destruction. A possible reason for the higher accuracy in the wrist joints is that the wrist joints had less class imbalance. For the PIP-IP, MCP, and CMC-M joints, prediction performance may be improved by increasing the number of non-intact cases.

The best-performing classification model was the MIMO local model; in particular, it shows better classification performance regarding F-measure and PR-AUC than the orthopedic surgeons for all joints in the case of erosion. As for JSN, general orthopedic surgeons are more familiar with evaluating it than erosion because they treat several diseases (such as osteoarthritis) for which evaluating JSN is meaningful. Thus, their performance for JSN was better than erosion. Despite such a situation, the MIMO local model is slightly better than the average of the orthopedic surgeons for all joints in the case of JSN. Erosion is more important than JSN in diagnosing RA [42]. Therefore, it has a clinical significance that the MIMO local model performed better than the orthopedic surgeons in the case of erosion. We thus conclude that the MIMO local model has a higher classification ability than the orthopedic surgeons in the case of erosion.

The limitations of this study are that we could use a relatively small number of hand data. More data may improve classification performance in the case of mild bone destruction in finger joints. If we have feet data, its combination with hand data would be helpful, especially for early diagnosis of RA [46].

In future work, we aim to improve classification performance by incorporating time-series information into the classification models, which is helpful for SHS scoring [9, 47]. Using the same framework as the MIMO local model will make it possible to incorporate time-series information.

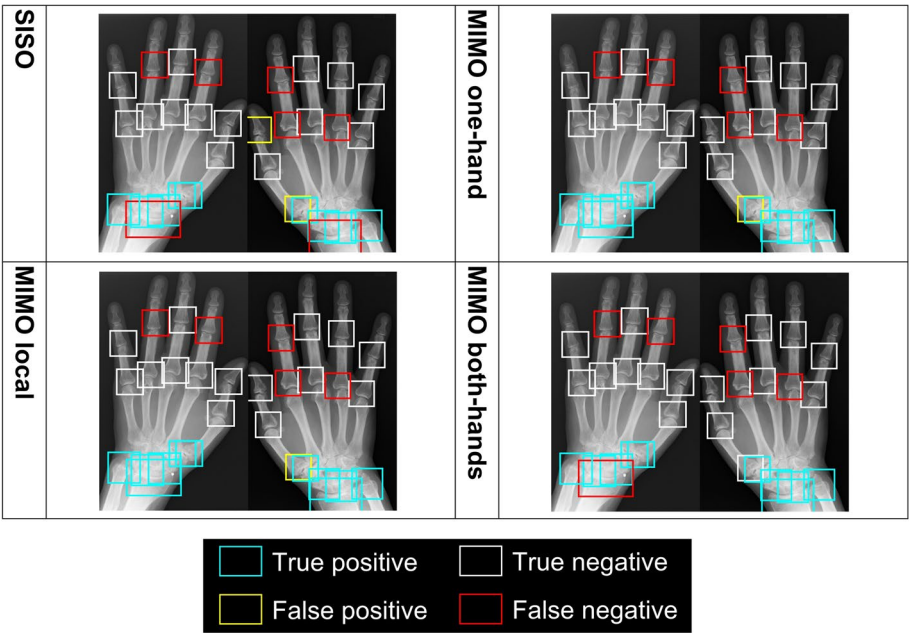


Fig. 8 The difficult case of erosion for all four classification models. Each bounding box represents the detected target joints. The color of the bounding box indicates how the classification results compare to ground-truth (GT). Blue indicates GT is non-intact, and prediction is non-intact (true positive). White indicates GT is intact, and prediction is intact (true negative). Yellow indicates GT is intact, and prediction is non-intact (false positive). Red indicates GT is non-intact, and prediction is intact (false negative). GT, ground-truth; SISO, single-input single-output; MIMO, multiple-input multiple-output

Conclusions

In conclusion, the proposed automatic-bone-destruction-evaluation system was effective. As for automatic detection, all the target joints were detected with high accuracy. As for automatic binary classification, the proposed classification method, which could compare the same contralateral joint, showed good classification performance for both erosion and JSN. In addition, the classification performance by the proposed method was better than that of the three orthopedic surgeons for erosion.

Abbreviations

AI: Artificial intelligence; CMC: Carpometacarpal; CMC-M: Carpometacarpal joint of the thumb and multangular; DNN: Deep neural networks; GT: Ground-truth; IP: Interphalangeal; JSN: Joint space narrowing; MCP: Metacarpophalangeal; MIMO: Multiple-input multiple-output; PIP: Proximal interphalangeal; RA: Rheumatoid arthritis; SHS: Modified Sharp/van der Heijde score; SISO: Single-input single-output.

Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s13075-022-02914-7>.

Additional file 1: Table S1. Final settings of hyperparameters (erosion). Each classification model's final settings of hyperparameters for each target joint are shown. "Wrist" represents the navicular, the lunate, the radius, and the ulna. Note: FC, fully connected; PIP, proximal interphalangeal; IP,

interphalangeal; MCP, metacarpophalangeal; CMC-M, carpometacarpal joint of the thumb and multangular.

Additional file 2: Table S2. Final settings of hyperparameters (JSN). Each classification model's final settings of hyperparameters for each target joint are shown. "Wrist" represents the multangular-navicular, the capitate-navicular-lunate, and the radiocarpal joint. Note: JSN, joint space narrowing; FC, fully connected; PIP, proximal interphalangeal; MCP, metacarpophalangeal; CMC, carpometacarpal.

Acknowledgments

The authors gratefully acknowledge Shota Harada, Kazuya Nishimura, and Kengo Araki for their great help in preparing the manuscript.

Authors' contributions

All authors contributed to the study conception and design. KM, SI, KK, MK, SA, TU, and YN collected the data. KM, RB, and SU wrote the manuscript, which was read and approved by all authors.

Funding

This study was supported by the Grants-in-Aid for Scientific Research of Japan Society for the Promotion of Science, Grant Number 19K09652.

Availability of data and materials

The data that support the findings of this study are available from the corresponding author, KM, upon reasonable request.

Declarations

Ethics approval and consent to participate

Ethical approvals for this study were obtained from the institutional review boards of all nine participating institutions.

Consent for publication

Not applicable.

Competing interests

The authors declare no competing interests.

Author details

¹Department of Orthopaedic Surgery, Graduate School of Medical Sciences, Kyushu University, 3-1-1 Maidashi, Higashi-Ku, Fukuoka 812-8582, Japan.

²Department of Advanced Information Technology, Kyushu University, 744 Motoooka, Nishi-Ku, Fukuoka 819-0395, Japan.

Received: 5 August 2022 Accepted: 25 September 2022

Published online: 03 October 2022

References

- Salaffi F, Carotti M, Carlo M. Conventional radiography in rheumatoid arthritis: new scientific insights and practical application. *Int J Clin Exp Med*. 2016;9:17012–27.
- Devauchelle Pensec V, Saraux A, Berthelot JM, Alapetite S, Chalès G, Le Henaff C, et al. Ability of hand radiographs to predict a further diagnosis of rheumatoid arthritis in patients with early arthritis. *J Rheumatol*. 2001;28:2603–7.
- Drosos AA, Pelechas E, Voulgari PV. Conventional radiography of the hands and wrists in rheumatoid arthritis. What a rheumatologist should know and how to interpret the radiological findings. *Rheumatol Int*. 2019;39:1331–41 Springer Science and Business Media LLC.
- McQueen FM. Imaging in early rheumatoid arthritis. *Best Pract Res Clin Rheumatol*. 2013;27:499–522.
- van der Heijde DM, van Riel PL, Nuver-Zwart IH, Gribnau FW, van de Putte LB. Effects of hydroxychloroquine and sulphasalazine on progression of joint damage in rheumatoid arthritis. *Lancet*. 1989;1:1036–8.
- Wen J, Liu J, Xin L, Wan L, Jiang H, Sun Y, et al. Effective factors on Sharp Score in patients with rheumatoid arthritis: a retrospective study. *BMC Musculoskelet Disord*. 2021;22:865.
- Mochizuki T, Yano K, Ikari K, Hiroshima R, Sakuma Y, Momohara S. Correlation between hand bone mineral density and joint destruction in established rheumatoid arthritis. *J Orthop*. 2017;14:461–5.
- Brown LE, Frits ML, Iannaccone CK, Weinblatt ME, Shadick NA, Liao KP. Clinical characteristics of RA patients with secondary SS and association with joint damage. *Rheumatology*. 2015;54:816–20.
- van der Heijde DMFM. Plain X-rays in rheumatoid arthritis: overview of scoring methods, their reliability and applicability. *Baillieres Clin Rheumatol*. 1996;10:435–53.
- Brower AC. Use of the radiograph to measure the course of rheumatoid arthritis. *Arthritis Rheum*. 1990;33:316–24 Wiley.
- Matsuno H, Yudoh K, Hanyu T, Kano S, Komatsubara Y, Matsubara T, et al. Quantitative assessment of hand radiographs of rheumatoid arthritis: interobserver variation in a multicenter radiographic study. *J Orthop Sci*. 2003;8:467–73 Elsevier BV.
- Hirano T, Nishide M, Nonaka N, Seita J, Ebina K, Sakurada K, et al. Development and validation of a deep-learning model for scoring of radiographic finger joint destruction in rheumatoid arthritis. *Rheumatol Adv Pract*. 2019;3:rkz047.
- Nakatsu K, Morita K, Yagi N, Kobashi S. Finger joint detection method in hand X-ray radiograph images using statistical shape model and support vector machine. In: 2020 International Symposium on Community-centric Systems (Ccs); 2020. p. 1–5.
- Nakatsu K, Chan P, Nii M, Nakagawa N, Kobashi S. Finger joint detection method for the automatic estimation of rheumatoid arthritis progression using machine learning. In: 2018 IEEE International Conference on Systems, Man, and Cybernetics (SMC). IEEE; 2018. p. 1315–20.
- Mathis A, Mamidanna P, Cury KM, Abe T, Murthy VN, Mathis MW, et al. DeepLabCut: markerless pose estimation of user-defined body parts with deep learning. *Nat Neurosci*. 2018;21:1281–9.
- Halla JT, Fallahi S, Hardin JG. Small joint involvement: a systematic roentgenographic study in rheumatoid arthritis. *Ann Rheum Dis*. 1986;45:327–30.
- Zangger P, Keystone EC, Bogoch ER. Asymmetry of small joint involvement in rheumatoid arthritis: prevalence and tendency towards symmetry over time. *Joint Bone Spine*. 2005;72:241–7.
- Sommer OJ, Kladosek A, Weiler V, Czembirek H, Boeck M, Stiskal M. Rheumatoid arthritis: a practical guide to state-of-the-art imaging, image interpretation, and clinical implications. *Radiographics*. 2005;25:381–98.
- Ory PA. Interpreting radiographic data in rheumatoid arthritis. *Ann Rheum Dis*. 2003;62:597–604.
- Fries JF, Bloch DA, Sharp JT, McShane DJ, Spitz P, Bluhm GB, et al. Assessment of radiologic progression in rheumatoid arthritis. A randomized, controlled trial. *Arthritis Rheum*. 1986;29:1–9.
- Ferrara R, Priolo F, Cammisà M, Bacarini L, Cerase A, Pasero G, et al. Clinical trials in rheumatoid arthritis: methodological suggestions for assessing radiographs arising from the GRISAR study. *Ann Rheum Dis*. 1997;56:608–12 BMJ Publishing Group Ltd.
- Hulsmans HM, Jacobs JW, van der Heijde DM, van Albada-Kuipers GA, Schenk Y, Bijlsma JW. The course of radiologic damage during the first six years of rheumatoid arthritis. *Arthritis Rheum*. 2000;43:1927–40.
- Scott DL, Coulton BL, Popert AJ. Long term progression of joint damage in rheumatoid arthritis. *Ann Rheum Dis*. 1986;45:373–8.
- Buda M, Maki A, Mazurowski MA. A systematic study of the class imbalance problem in convolutional neural networks. *Neural Netw*. 2018;106:249–59 Elsevier.
- Simonyan K, Zisserman A. Very deep convolutional networks for large-scale image recognition. *ICLR*; 2015. Available from: <https://www.semanticscholar.org/paper/eb42cf88027de515750f230b23b1a057dc782108>.
- Li Z, Liu F, Yang W, Peng S, Zhou J. A survey of convolutional neural networks: analysis, applications, and prospects. *IEEE Trans Neural Netw Learn Syst*. 2021. <http://dx.doi.org/10.1109/TNNLS.2021.3084827>.
- Deng J. ImageNet: A LARGE-SCALE hierarchical image database. *Proc IEEE Comput Soc Conf Comput Vis Pattern Recognit*. 2009. Available from: <https://ci.nii.ac.jp/naid/10027363646>.
- Guo Y, Shi H, Kumar A, Grauman K, Rosing T, Feris R. Spottune: transfer learning through adaptive fine-tuning. In: *Proceedings of the IEEE/CVF Conference on Computer Vision and Pattern Recognition*. openaccess.thecvf.com; 2019. p. 4805–14.
- Tougui I, Jilbab A, Mhamdi JE. Impact of the choice of cross-validation techniques on the results of machine learning-based diagnostic applications. *Healthc Inform Res*. 2021;27:189–99 synapse.koreamed.org.
- Ying X. An overview of overfitting and its solutions. *J Phys Conf Ser*. 2019;1168:022022 IOP Publishing.
- Basha SHS, Dubey SR, Pulabaigari V, Mukherjee S. Impact of fully connected layers on performance of convolutional neural networks for image classification. *Neurocomput*. 2020;378:112–9 Elsevier.
- He K, Zhang X, Ren S, Sun J. Delving deep into rectifiers: surpassing human-level performance on ImageNet classification. In: 2015 IEEE International Conference on Computer Vision (ICCV); 2015. p. 1026–34.
- Srivastava N, Hinton G, Krizhevsky A, Sutskever I, Salakhutdinov R. Dropout: a simple way to prevent neural networks from overfitting. *J Mach Learn Res*. 2014;15:1929–58.
- Radiuk PM. Impact of training set batch size on the performance of convolutional neural networks for diverse datasets. *Inf Technol Manag Sci*. 2017;20. Riga Technical University. Available from: <http://elar.khmnu.edu.ua/handle/123456789/11047>.
- Ruby U, Yendapalli V. Binary cross entropy with deep learning technique for image classification. *J Adv Trends Comput*. . 2020. [researchgate.net](https://www.researchgate.net/profile/Vamsidhar-Yendapalli/publication/344854379_Binary_cross_entropy_with_deep_learning_technique_for_Image_classification/links/5f93eed692851c14bce1ac68/Binary-cross-entropy-with-deep-learning-technique-for-Image-classification.pdf). Available from: https://www.researchgate.net/profile/Vamsidhar-Yendapalli/publication/344854379_Binary_cross_entropy_with_deep_learning_technique_for_Image_classification/links/5f93eed692851c14bce1ac68/Binary-cross-entropy-with-deep-learning-technique-for-Image-classification.pdf.
- Kingma DP, Ba J. Adam: a method for stochastic optimization. *arXiv [cs.LG]*. 2014. Available from: <http://arxiv.org/abs/1412.6980>.
- Shorten C, Khoshgoftaar TM. A survey on image data augmentation for deep learning. *J Big Data*. 2019;6:60 Springer.
- Canbek G, Sagioglu S, Temizel TT, Baykal N. Binary classification performance measures/metrics: a comprehensive visualized roadmap to gain new insights. In: 2017 International Conference on Computer Science and Engineering (UBMK); 2017. p. 821–6. ieeexplore.ieee.org.

39. Keilwagen J, Grosse I, Grau J. Area under precision-recall curves for weighted and unweighted data. *PLoS One*. 2014;9:e92209 [journals.plos.org](https://doi.org/10.1371/journal.plosone.0092209).
40. Movahedi F, Padman R, Antaki J. Limitations of ROC on imbalanced data: evaluation of LVAD mortality risk scores. *ArXiv*. 2020. Available from: <https://www.semanticscholar.org/paper/3a83bb7335038801013f3805f09572c3f2f12280>.
41. Nan Y, Chai KM, Lee WS, Chieu HL. Optimizing F-measure: a tale of two approaches [Internet]. *arXiv [cs.LG]*. 2012. Available from: <http://arxiv.org/abs/1206.4625>.
42. van der Heijde D. Erosions versus joint space narrowing in rheumatoid arthritis: what do we know? *Ann Rheum Dis*. 2011;70(Suppl 1):i1 16–8.
43. Read GO, Solomon L, Biddulph S. Relationship between finger and wrist deformities in rheumatoid arthritis. *Ann Rheum Dis*. 1983;42:619–25.
44. Klarlund M, Ostergaard M, Jensen KE, Madsen JL, Skjødt H, Lorenzen I. Magnetic resonance imaging, radiography, and scintigraphy of the finger joints: one year follow up of patients with early arthritis. The TIRA Group. *Ann Rheum Dis*. 2000;59:521–8.
45. Guillemin F, Billot L, Boini S, Gerard N, Ødegaard S, Kvien TK. Reproducibility and sensitivity to change of 5 methods for scoring hand radiographic damage in patients with rheumatoid arthritis. *J Rheumatol*. 2005;32:778–86.
46. Visser H. Early diagnosis of rheumatoid arthritis. *Best Pract Res Clin Rheumatol*. 2005;19:55–72 Elsevier.
47. van der Heijde D, Boonen A, Boers M, Kostense P, van der Linden S. Reading radiographs in chronological order, in pairs or as single films has important implications for the discriminative power of rheumatoid arthritis clinical trials. *Rheumatology*. 1999;38:1213–20 Oxford Academic.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Ready to submit your research? Choose BMC and benefit from:

- fast, convenient online submission
- thorough peer review by experienced researchers in your field
- rapid publication on acceptance
- support for research data, including large and complex data types
- gold Open Access which fosters wider collaboration and increased citations
- maximum visibility for your research: over 100M website views per year

At BMC, research is always in progress.

Learn more biomedcentral.com/submissions

